



Vivek Maradia :: Center for Proton Therapy :: Paul Scherrer Institute

# Different methods for increasing transmission in cyclotron-based proton therapy facilities

09.12.2022 CYC 2022, Beijing, China



#### Pencil Beam Scanning proton therapy



https://4570book.info/amazing-cliparts/kopf-mensch-clipart-fish.html

https://de.depositphotos.com/130440300/stock-illustration-lungs-icon-in-outline-style.html



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#### Shorter field delivery times are advantageous



#### Problem with Energy degradation













#### Most of the facilities transports 30 pi\*mm\*mrad or less emittance





#### PROScan beamline









#### Transmission through degrader and ESS





Simulation model

# We have developed a simulation model in **BDSIM** and validated with our clinical tune.



	M1	M2	M3	Coupling point	isocenter
<b>BDSIM Simulation</b>	10 ± 0.3%	$1.47 \pm 0.04\%$	0.23 ± 0.007%	0.22 ± 0.007%	0.13 ± 0.004%
Measurements	10.1 ± 0.7%	1.46 ± 0.1%	0.21 ± 0.015%	0.21 ± 0.015%	0.13 ± 0.002%

V. Maradia et al 2021, Medical Physics





#### 1:1 imaging

Emittance : 30 pi\*mm\*mrad Beam size : 3 mm Divergence : 10 mrad Transmission : 57%



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Gantry beam optics



#### 1:1 imaging

Emittance : 30 pi\*mm\*mrad Transmission : 57%

V. Maradia et al 2021, IPAC Proceedings



#### **2:1 imaging**

Emittance : 30 pi\*mm\*mrad Transmission : 84%



#### Gantry beam optics with 2:1 imaging



V. Maradia et al 2022, Medical Physics



#### Gantry beam optics





### Use of *large beam size* & *small divergence* at gantry entrance together with *2:1 imaging* beam optics will allow to transport *100 π\*mm\*mrad* through gantry while having *60%* transmission.





#### PROScan beamline









#### We can transport higher emittance In y-plane compare to x-plane

To achieve gantry angle independent beam at isocenter, we need to have same emittance in both planes at gantry entrance.









 $\epsilon$ =67±2  $\pi$ \*mm\*mrad

V. Maradia et al 2022, Frontiers in Physics





**Distance from cyclotron [m]** 



#### For 70 MeV beam

#### Clinical beam optics : 0.13%

#### Scattering foil + 2:1 imaging : 0.4%

(1.8 times larger beam size)

# Gain : ~ factor 3 (Experimentally)











Y-axis: Beam size: 4 mm Divergence: 25 mrad

X-axis: Beam size: 10 mm Divergence: 10 mrad



Transmission gain with asymmetric collimator

#### For 70 MeV beam

#### Clinical beam optics : 0.13%

#### Asymmetric collimator + 2:1 imaging : 0.72%

(1.5 times larger beam size)

# Gain : ~ factor 6 (Simulation)







## 250 MeV -> 70 MeV -> dp/p = 4.5% dp/p = 0.4%



#### Gantry with momentum cooling capabilities

#### **Fixed beamline**

#### **Rotating beamline (Gantry)**





Transmission





#### Beam size and dose rate





#### For 70 MeV beam

#### Clinical beam optics : 0.13%

#### Momentum cooling + 2:1 imaging : 10%

(1.7 times larger beam size)

# Gain : ~ factor 80 (Simulation)





Overview of transmission improvement

#### For 70 MeV beam

Clinical beam optics : 0.13% Scattering foil + 2:1 imaging : factor 3 Asymmetric collimator + 2:1 imaging : factor 6 New gantry with momentum cooling : factor 80



#### Impact of the high transmission

Efficient treatment delivery for moving targets

Ultra-fast treatment delivery (treatment delivery in 5-10 sec)

Treatment of new indications with protons

Possible to achieve FLASH dose rates for all energy beams

Reduced shielding requirement (investment cost reduction by few M\$)



#### Wir schaffen Wissen – heute für morgen

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- Technical support group
- Radiation protection group

